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Towards predicting the stability of protein-stabilized emulsions

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ABSTRACT

The protein concentration is known to determine the stability against coalescence during formation of emulsions. Recently, it was observed that the protein concentration also influences the stability of formed emulsions against flocculation as a result of changes in the ionic strength. In both cases, the stability was postulated to be the result of a complete (i.e. saturated) coverage of the interface. By combining the current views on emulsion stability against coalescence and flocculation with new experimental data, an empiric model is established to predict emulsion stability based on protein molecular properties such as exposed hydrophobicity and charge. It was shown that besides protein concentration, the adsorbed layer (i.e. maximum adsorbed amount and interfacial area) dominates emulsion stability against coalescence and flocculation. Surprisingly, the emulsion stability was also affected by the adsorption rate. From these observations, it was concluded that a completely covered interface indeed ensures the stability of an emulsion against coalescence and flocculation. The contribution of adsorption rate and

23 adsorbed amount on the stability of emulsions was combined in a surface coverage model. For
24 this model, the adsorbed amount was predicted from the protein radius, surface charge and ionic
25 strength. Moreover, the adsorption rate, which depends on the protein charge and exposed
26 hydrophobicity, was approximated by the relative exposed hydrophobicity (Q_H). The model in
27 the current state already showed good correspondence with the experimental data, and was
28 furthermore shown to be applicable to describe data obtained from literature.

29

30 **KEYWORDS**

31 Coalescence, flocculation, model, adsorption rate, adsorbed amount, surface coverage

32

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60

61 **1. INTRODUCTION**

62 Proteins are widely used for the stabilization of emulsions [1-3]. The four main destabilization
63 mechanisms affecting a protein-stabilized emulsion are creaming, coalescence, flocculation and
64 Ostwald ripening [4]. During emulsion formation, proteins are typically considered to adsorb to
65 the interface, and thereby stabilize the emulsion against coalescence [5]. After formation, the
66 emulsion stability against flocculation is described to be determined by the charge of the
67 adsorbed protein layer [4, 6]. For oil-in-water emulsions destabilization by Ostwald ripening is

68 often neglected, since typical triglyceride oils used in food emulsions, such as corn and peanut
69 oil, have a low solubility in water [8-10] and can therefore not diffuse through the water phase.
70 Next, the link between coalescence and flocculation of emulsions and the protein molecular
71 properties are reviewed. Based on this information and recent work, an empiric model is
72 proposed that links the stability against coalescence and flocculation to the protein molecular
73 properties such as size, charge and hydrophobicity.

74

75 *1.1. Stability against coalescence*

76 Coalescence is reported to be the main destabilization mechanism during emulsion formation [5].
77 During formation, droplets with a certain defined size ($d_{3,2, \min}$) will be formed, depending on for
78 instance power input, interfacial tension and mass density of the continuous phase [7]. If
79 sufficient protein is present to cover the newly formed interface (i.e. emulsion droplet)
80 completely, the droplets are considered to be stable ($d_{3,2} = d_{3,2, \min}$) (figure 1A). A lack of protein
81 in the continuous phase will lead to incomplete coverage of the interface. This in turn results in
82 coalescence during formation, until an interfacial area (i.e. droplet size) is reached for which
83 there is sufficient protein present (figure 1A). Coalescence can therefore be prevented by
84 increasing the protein concentration in the continuous phase. This explains the two characteristic
85 concentration regimes which are observed during emulsion formation (i.e. protein-poor and
86 protein-rich regime) [2, 11].

87 In the protein-poor regime (regime I), the droplet size ($d_{3,2}$) is equal to the minimal droplet size
88 for which the complete interface can be (sufficiently) covered with protein, as described in
89 equation 1 [11]. The maximum adsorbed amount (Γ_{\max}) in this regime corresponds closely to that
90 of a monolayer [2, 12, 13]. Consequently, if the droplet size, calculated from equation 1 [11], is

91 plotted against protein concentration, different curves are obtained depending on volume fraction
 92 oil (Φ_{oil}) and Γ_{max} (figure 2A). Recently, the maximum adsorbed amount for a protein has
 93 recently been described to be influenced by its molecular properties (i.e. size and charge) and
 94 system conditions (i.e. ionic strength) [14], as was previously shown for hard-sphere colloids
 95 [15-17].

96 In the protein-rich regime (regime II), the droplet size is only affected by factors such as power
 97 input, interfacial tension and mass density of the continuous phase ($d_{3,2} = d_{3,2, min}$) (equation 2).

$$d_{3,2(I)} \approx \frac{6\Phi_{oil}\Gamma_{max}}{(1-\Phi_{oil})C} \quad (1)$$

$$d_{3,2(II)} = d_{3,2, min} \quad (2)$$

98 where Φ_{oil} is the volume fraction oil [-], Γ_{max} is the maximum adsorbed amount [$mg\ m^{-2}$] and C
 99 is the protein concentration [$g\ L^{-1}$].

100 Assuming the validity of equations 1 and 2, all curves are expected to superimpose onto a single
 101 curve by correcting for the C, Φ_{oil} and Γ_{max} (figure 2B). In this curve one critical point (F_s) is
 102 identified, where all curves shift from the protein-poor to the protein-rich regime. Using this
 103 stability factor (i.e. F_s), the critical protein concentration (C_{cr}) for any Φ_{oil} and Γ_{max} can be
 104 calculated by replacing the $d_{3,2}$ with the $d_{3,2, min}$ of the system. In addition to these parameters (i.e.
 105 C, Φ_{oil} and Γ_{max}), the shift between the protein-poor and protein-rich regime, and thereby C_{cr} , has
 106 recently been reported to depend on the exposed hydrophobicity (Q_H) [18]. This was postulated
 107 to be caused by the fact that an increase of Q_H decreases the barrier for adsorption to the air-
 108 water interface, resulting in a higher adsorption rate [14, 19]. The maximum adsorbed amount at
 109 the air-water and the oil-water interface has, on the other hand, been described to be independent
 110 of the exposed hydrophobicity of the protein [14, 19, 20]. A higher adsorption rate therefore
 111 translates into faster coverage of the interface. This helps to prevent coalescence during

112 formation, and is consequently expected to result in the formation of smaller droplets under
113 similar conditions. Accordingly, the adsorption rate has recently been proposed to affect the
114 initial droplet size of emulsions stabilized by surfactants and proteins [21]. In summary, the
115 critical concentration is expected to decrease with increasing exposed hydrophobicity due to an
116 increase of the adsorption rate (k_{adsorb}). Therefore, it is proposed that equation 1 for the protein-
117 poor regime can be approximated by equation 3.

$$d_{3,2(l)} \approx \frac{6\Phi_{oil}\Gamma_{\max}}{(1-\Phi_{oil})Ck_{\text{adsorb}}} \quad (3)$$

118 The importance of adsorption rate, even under turbulent flow, is demonstrated by the fact that
119 Gum Arabic, which is described to adsorb slower to the oil-water interface than β -lactoglobulin
120 [22], was described to form larger emulsions droplets than WPI at an equal concentration [23,
121 24].

122

123 1.2. *Stability against flocculation*

124 Flocculation is reported to be the main destabilization mechanism during emulsion stabilization
125 [6, 20]. The occurrence of flocculation has often been explained based on the interactions (e.g.
126 electrostatic repulsion) between emulsion droplets [4, 6, 25]. In case of net repulsive interactions
127 (i.e. at a pH away from the iso-electric point (pI) and at low ionic strength), the electrostatic
128 repulsion between the adsorbed layer as a result of protein charge prevents flocculation. If the
129 charge decreases (i.e. shift of pH towards pI and/or an increase of the ionic strength), the
130 electrostatic repulsion decreases and the emulsion droplets may flocculate. However, recent
131 experiments have indicated that not only the inter-droplet interactions, but also the adsorbed
132 amount changes with conditions (i.e. ionic strength) [14, 26]. A change in adsorbed amount latter
133 was also observed for particle [15-17] and protein adsorption [27-29] at solid-liquid interfaces.

134 The maximum adsorbed amount (Γ_{\max}) was shown to increase with increasing ionic strength due
135 to a decrease of the effective radius of the protein (as a result of a decrease of the Debye
136 screening length) [17, 30-33]. Therefore, more protein is needed to reach the maximum
137 adsorbed amount and completely cover the interface. At higher protein concentrations, more
138 protein is present to supplement a partially covered interface, thereby resulting in an increased
139 stability against flocculation [18, 20] (figure 1B). This shows that both the stability during
140 formation (figure 1A) and after changes in the conditions (figure 1B) increases with increasing
141 protein concentration. It is, therefore, postulated that equation 3, which accounts for the adsorbed
142 amount (Γ_{\max}) at the interface, describes the stability during formation, as well as the stability
143 after changes in conditions.

144

145 *1.3. Theoretical prediction of the maximum adsorbed amount*

146 The maximum adsorbed amount was shown to be an important factor affecting the
147 emulsion stability against coalescence and flocculation. Therefore, it is of interest to
148 quantitatively predict the adsorbed amount for different proteins under different
149 conditions. Recently, the Random Sequential Adsorption (RSA) model with the effective
150 hard-particle concept [34-36] was successfully applied to describe Γ_{\max} for globular
151 proteins at the air-water interface [14]. The theoretical maximum adsorbed amount for a
152 close-packed monolayer ($\Gamma_{\text{mono, theory}}$) was predicted using equation 4 [14]. In accordance
153 with the RSA model, this prediction describes globular proteins as hard disks adsorbing at
154 a two-dimensional interface. At the jamming limit, the saturation coverage (θ_{∞}) is
155 approximated to be 0.547 [30, 37-39].

$$\Gamma_{mono,theory} = \frac{10^3 M_w}{\pi R_{eff}^2 N_a} \theta_{\infty} \quad (4)$$

156 in which $\Gamma_{mono, theory}$ is the theoretical maximum adsorbed amount of a close-packed
 157 monolayer [mg m^{-2}], M_w is the molecular mass of the protein [g mol^{-1}], R_{eff} is the
 158 effective hard-sphere radius of an adsorbed protein [m], N_a is the Avogadro constant
 159 [$6.022 \times 10^{23} \text{ mol}^{-1}$] and θ_{∞} is the saturation coverage, which has a value of 0.547 for
 160 irreversible bound, non-diffusing particles [30, 37-39].

161 The RSA model was originally developed for the adsorption of hard sphere, non-
 162 interacting particles [40]. Later, the effective hard-sphere particle concept was introduced
 163 to account for interacting particles [34-36]. The validity of the latter concept to describe
 164 Γ_{max} of globular proteins indicates that adsorbed globular proteins can be depicted as hard
 165 sphere particles with a soft shell as a result of their charge. The effective radius of a
 166 charged particle (i.e. globular protein) adsorbed at an interface can be estimated by the
 167 hard-sphere approximation as the sum of the protein radius (R_p) and a characteristic
 168 distance due to electrostatic repulsion [17, 30-33] (equation 5) [14]. Assuming a constant
 169 surface charge, the effective radius (R_{eff}) can be described by equation 6 [14].

$$R_{eff} = R_p - \frac{1}{2} \ln \left(\frac{U_{driving}}{2\pi\epsilon_0\epsilon_r R_p \Psi_0^2} \right) \kappa^{-1} \quad (5)$$

$$R_{eff} = R_p - \frac{1}{2} \ln \left(\frac{x}{R_p} \right) \kappa^{-1} \quad (6)$$

170 where R_p is the protein radius [m], $U_{driving}$ is the adsorption driving interaction [J], ϵ_0 is
 171 the dielectric constant of a vacuum [$8.85 \times 10^{-12} \text{ C}^2 \text{ J}^{-1} \text{ m}^{-1}$], ϵ_r is the relative dielectric
 172 constant of the medium [80], Ψ_0 is the surface potential [V], κ^{-1} is the Debye screening
 173 length [m] and x is a constant [m]. The constant was found to be $1.77 \times 10^{-9} \text{ m}$ for

174 β -lactoglobulin and ovalbumin and 0 m for lysozyme at pH 7.0 [14]. The radius of a
175 globular protein and the Debye screening length can be calculated using equations 7 [41]
176 and 8 [42], respectively.

$$R_p = \left(\frac{3vM_w}{4\pi N_a} \right)^{\frac{1}{3}} \quad (7)$$

$$\kappa^{-1} = \sqrt{\frac{2N_a e^2 I}{\epsilon_0 \epsilon_r k_B T}} \quad (8)$$

177 in which v is the partial specific volume [$0.73 \times 10^{-6} \text{ m}^3 \text{ g}^{-1}$] [41], e is the elementary
178 charge [$1.602 \times 10^{-19} \text{ C}$], I is the ionic strength [mol m^{-3}], k_B is the Boltzmann constant
179 [$1.38 \times 10^{-23} \text{ J K}^{-1}$] and T is the temperature [K].

180 It is important to realize that the RSA model assumes that: 1) particles adsorb randomly
181 on the interface, depending on the fact whether or not they encounter an empty spot. 2)
182 adsorbed particles do not desorb from the interface; 3) adsorbed particles do not diffuse
183 on the interface [43]. For globular proteins, the first two assumptions have been validated
184 [44], whereas the latter can be debated. Two limitations of the RSA model are that it does
185 not account for multilayer adsorption and unfolding at the interface. The validity of the
186 model for globular proteins means that, under the tested conditions, the structural changes
187 upon adsorption are not significant and that the proteins do not form multilayers. This is
188 in contrast with commonly held views that proteins unfold at interfaces [45, 46] and may
189 form multilayers [5]. Several studies, however, suggested that protein unfolding at the
190 interface is concentration dependent [47, 48]. At low protein concentrations, the timescale
191 of adsorption is slower than the timescale of unfolding and spreading. At higher protein
192 concentrations, the opposite is the case (i.e. the timescale of adsorption is faster than the
193 timescale of unfolding and spreading), thereby preventing unfolding and spreading. For

194 β -lactoglobulin at the air-water interface, no effect of protein concentration on the
195 adsorbed amount was observed at concentrations exceeding 0.1 g L^{-1} [49], showing that
196 unfolding becomes negligible above this concentration. At the same time, to form an
197 emulsion or foam, a certain minimal amount of protein needs to adsorb within the
198 timescale of formation. Consequently, in each case where adsorption is sufficiently fast,
199 the protein concentration will be so high that it is even in the consensus view unlikely for
200 proteins to significantly unfold.

201

202 *1.4. Towards an empiric model for emulsion stability*

203 The previous, especially equation 3, indicates that it should be possible to describe and to predict
204 emulsion stability based the adsorption rate and the adsorbed amount. Therefore, the aim of this
205 study is to confirm this view with new experimental data, and to establish a first empiric model.
206 To accomplish this, the effect and contribution of C , Γ_{\max} and k_{adsorb} on emulsion stability was
207 studied for different proteins at various ionic strengths.

208

209 **2. MATERIALS AND METHODS**

210 *2.1. Materials*

211 Lysozyme (Lys; L6876, Lot n° 051K7028; purity > 90 % based on size-exclusion
212 chromatography), β -lactoglobulin (β -lg; L0130, Lot n° SLBC2933V; protein content of
213 99 % (N x 6.38), of which 94 % β -lactoglobulin based on SDS-PAGE) and ovalbumin
214 (Ova; A5503 Lot n° 031M7008V; protein content of 98 % (N x 6.22), of which 92 %
215 ovalbumin based on agarose gel electrophoresis) were purchased from Sigma-Aldrich (St.

216 Louis, MO, USA). All other chemicals were of analytical grade and purchased from
217 either Sigma-Aldrich or Merck (Darmstadt, Germany).

218

219 2.2. *Quantification of exposed hydrophobicity*

220 The increase in fluorescence intensity upon binding of 8-anilino-1-naphthalenesulfonic
221 acid (ANSA) to the accessible hydrophobic regions of the protein is used as a measure of
222 the protein surface hydrophobicity [50]. The proteins were dissolved in 10 mM sodium
223 phosphate buffer pH 7.0 in a concentration of 0.1 g L⁻¹. The measurements were
224 performed on a Varian Cary Eclipse fluorescence spectrophotometer (Agilent
225 Technologies, Santa Clara, CA, USA) as described elsewhere [14].

226

227 2.3. *Zeta potential of protein solutions*

228 Zeta potentials of the proteins in solution were determined with a Zetasizer Nano ZSP
229 (Malvern Instruments, Worcestershire, UK) using the laser Doppler velocimetry
230 technique. The proteins (10 g L⁻¹) were dissolved in 10 mM sodium phosphate buffer pH
231 7.0. The measurements were performed at 25 °C and 40 Volt. The results of five
232 sequential runs were averaged. Zeta potentials were calculated with Henry's equation [51]
233 (equation 9).

$$\zeta = \frac{3\eta\mu_e}{2\varepsilon F(\kappa\alpha)} \quad (9)$$

234 in which ζ is the zeta potential [V], η is the viscosity [0.8872 x 10⁻³ Pa s], μ_e is the
235 electrophoretic mobility [m² V⁻¹ s⁻¹], ε is the dielectric constant of the medium [7.08 x
236 10⁻¹⁰ C² J⁻¹ m⁻¹] and $F(\kappa\alpha)$ is Henry's function [-], which equals 1.5 using the
237 Smoluchowski approximation [51].

238 2.4. *Emulsification*

239 The protein solutions were mixed with 10 %(v/v) sunflower oil. A pre-emulsion was
240 prepared using an Ultra turrax Type T-25B (IKA, Staufen, Germany) at 9500 rpm for 1
241 min. Subsequently, the pre-emulsion was passed 30 times through a Labhoscope 2.0
242 laboratory scale high-pressure homogenizer (Delta Instruments, Drachten, The
243 Netherlands) operated at 15 MPa. The solutions were cooled on ice-water during
244 homogenization. Three different sets of experiments were performed:

245 2.4.1. Effect of protein concentration

246 β -Lactoglobulin was dissolved in 10 mM sodium phosphate buffer pH 7.0 at
247 concentrations of 1, 2, 2.5, 3, 4, 5, 7.5 and 10 g L⁻¹.

248 2.4.2. Effect of ionic strength

249 β -Lactoglobulin was dissolved in 10 mM sodium phosphate buffer pH 7.0 in the absence
250 or presence of 20 and 190 mM NaCl at concentrations of 1, 2, 2.5, 3, 4, 5, 7.5 and 10
251 g L⁻¹. Moreover, the ionic strength of the β -lactoglobulin emulsions prepared in the
252 absence of NaCl was adjusted to 30 and 200 mM with 2 M NaCl after emulsification.

253 2.4.3. Effect of adsorption rate (k_{adsorb})

254 β -Lactoglobulin, ovalbumin and lysozyme were dissolved in 10 mM sodium phosphate
255 buffer pH 7.0 at concentrations of 1, 2, 2.5, 3, 4, 5, 7.5 and 10 g L⁻¹, 1, 2.5, 5, 7.5, 10, 15
256 and 20 g L⁻¹ and 2.5, 5, 10, 15, 20, 25 g L⁻¹, respectively.

257 Subsequently, the emulsions were stored for 24 hours at 20 °C prior to further analysis.
258 For selected samples, it was confirmed that no significant changes occurred during this
259 storage period.

260

261 2.5. *Zeta potential of emulsion droplets*

262 Zeta potentials of the emulsion droplets were determined with a Zetasizer Nano ZS
263 (Malvern Instruments) using the laser Doppler velocimetry technique. The emulsions
264 were diluted 500 times to prevent multiple scattering. The measurements were performed
265 at 25 °C and 40 Volt. The results of five sequential runs were averaged. Zeta potentials
266 were calculated with Henry's equation [51] (equation 9).

267

268 2.6. *Determination of droplet size*

269 2.6.1. Diffusing wave spectroscopy (DWS)

270 As indication of the droplet size *in situ*, without dilution, DWS measurements were
271 performed as described previously [52]. The autocorrelation function was averaged from
272 five sequential runs of 120 seconds. Subsequently, the autocorrelation functions were
273 normalized by dividing the obtained $g_2(t)-1$ values by the maximum measured value.
274 Normalized autocorrelation functions were then fitted using equation 11. This was
275 derived from Ruis et al. [52], assuming that $\langle \Delta r^2(t) \rangle = 6Dt^p$ for $p < 1 = \alpha t^x$ for $x < 1$.

$$g_2(t) - 1 \approx (e^{-\langle \Delta r^2(t) \rangle})^2 \approx e^{-\alpha t^x} \quad (11)$$

276 The decay time ($\tau_{1/2}$), which is defined as the time at which $g_2(t)-1$ decayed to half of its
277 initial value, was determined using the fitted equation. An increase of the decay time is
278 related to decreased droplet mobility [53, 54]. Although DWS in the tested regime
279 (droplet size and Φ) has been described to be suitable for sizing [55], the droplet mobility
280 is only used as an indication of the droplet size.

281

282

283 2.6.2. Laser diffraction

284 The average droplet size of the emulsions was measured using laser light diffraction
285 (Mastersizer 2000, Malvern Instruments) equipped with a Hydro SM sample dispersion
286 unit. The droplet size was calculated using the general purpose model with a refractive
287 index of 1.45 and 1.33 for the droplet and continuous phase, respectively. The volume-
288 surface average diameter ($d_{3,2}$) (equation 10) was reported as an average of at least five
289 runs.

$$d_{3,2} = \frac{\sum N_i d_i^3}{\sum N_i d_i^2} \quad (10)$$

290 in which N_i and d_i represent the number and diameter of droplets of size class i , respectively.

291

292 **3. RESULTS AND DISCUSSION**

293 *3.1. Colloidal model*

294 Based on a simplified colloidal model (i.e. DLVO interactions), it is expected that
295 flocculation of emulsion droplets with a similar radius would occur when the zeta
296 potential of the emulsion droplets decreases below a certain critical value (i.e. decrease of
297 the electrostatic repulsion) [42]. As expected, an increase of the ionic strength (i.e.
298 decrease of zeta potential) destabilizes the emulsion with a low protein concentration (in
299 this case 2 g L⁻¹). This resulted in flocculation as indicated by a longer decay time ($\tau_{1/2}$),
300 as measured by DWS (figure 3).

301 An increase of the ionic strength leads to a similar decrease of the zeta potential of the
302 emulsion with a higher protein concentration (in this case 5 g L⁻¹). Surprisingly, the
303 decrease does not lead to salt-induced flocculation for this emulsion. This observation is
304 explained by the fact that at an increased ionic strength more protein is needed to

305 completely cover the interface. The emulsion with a low protein concentration cannot
306 comply with the need for protein (i.e. protein-poor regime). As a result, the interface
307 cannot be completely covered, leading to flocculation of emulsion droplets. If sufficient
308 protein is present in the continuous phase (i.e. at 5 g L^{-1} ; protein-rich regime), the excess
309 protein adsorbs to the bare interface and stabilizes the emulsion against flocculation. This
310 proposed view is referred to as the surface coverage model.

311 To confirm that this stabilizing effect results from an increase of the protein
312 concentration, the protein concentration of the emulsion prepared at 2 g L^{-1} is
313 supplemented to a final concentration of 5 g L^{-1} . As expected, this also results in an
314 emulsion which is stable against salt-induced flocculation. It is therefore concluded that
315 adsorbed layer, as considered in the surface coverage model, is of importance for the
316 stability of the emulsions. This is in line with previous studies showing the importance of
317 excess protein in the continuous phase for the stability against salt-induced flocculation
318 [18, 20].

319 A similar behaviour was observed for emulsions prepared in the presence of NaCl and for
320 emulsions of which the ionic strength was adjusted after emulsification. This shows the
321 analogy between emulsion formation and stabilization. Moreover, it confirms that, as
322 described in the surface coverage model, the protein concentration relative to the
323 adsorbed amount and interfacial area is important for both processes (as described by
324 equations 1 and 3).

325

326

327

328 3.2. *Surface coverage model*

329 Based on the above, the stability of a protein-stabilized emulsion during formation and
330 after changes in system conditions can be considered to be determined by the fact whether
331 the protein covers the interface completely. Since interfacial coverage is thought to be the
332 dominant factor, it will be referred to as the surface coverage model. However, so far the
333 model only comprises of a view, validated by some qualitative experimental results. In a
334 first approach, the effect of molecular properties and system conditions on emulsion
335 stability during formation (i.e. stability against coalescence) was studied to come to an
336 empiric model.

337 3.2.1. Effect of adsorption rate (k_{adsorb})

338 To determine the effect of the adsorption rate (at a constant ionic strength of 10 mM), the
339 decay time and average droplet size of emulsions stabilized by three different proteins
340 (lysozyme, ovalbumin and β -lactoglobulin) was determined. This shows that the critical
341 protein concentration (C_{cr}), which marks the transition from the protein-poor to the
342 protein-rich regime, shifts from $\geq 25 \text{ g L}^{-1}$ for lysozyme to $\sim 10 \text{ g L}^{-1}$ for ovalbumin and 2
343 g L^{-1} for β -lactoglobulin (figure 4A). This difference is also reflected in the average
344 droplet size ($d_{3,2}$) at 5 g L^{-1} which varies from $7.33 \mu\text{m}$ for lysozyme to 0.50 and $0.26 \mu\text{m}$
345 for ovalbumin and β -lactoglobulin, respectively (figure 4B). Based on equation 1, the
346 difference between the proteins can be explained by a shift of the maximum adsorbed
347 amount (Γ_{max}). To test this, curves were plotted as described by equation 1, using Γ_{max}
348 calculated assuming a full monolayer coverage ($\Gamma_{\text{mono, theory}}$) predicted by a model
349 described previously [14] (table 1). After this correction, the curves of the different
350 proteins do still not superimpose (figure 4C). This shows that the observed differences

351 between the proteins cannot only be explained by differences in adsorbed amount.
352 Therefore, the initial adsorption rate (k_{adsorb}) is included as described in equation 3. At a
353 given concentration and ionic strength, the adsorption rate was described to increase with
354 increasing relative exposed hydrophobicity [14, 49]. Therefore, the relative exposed
355 hydrophobicity of the protein (Q_{H}) was used as an indication for k_{adsorb} (table 1).
356 When corrected for Q_{H} , all curves superimpose (figure 4D). All emulsions above the
357 stability factor (F_{s}) of 2 are in the protein-rich regime. This confirms that the critical
358 protein concentration is also affected by the initial adsorption rate (i.e. affinity of the
359 protein towards adsorption to the interface).

360 3.2.2. Effect of adsorbed amount (Γ_{max})

361 To determine the effect of the adsorbed amount, the droplet size of emulsions stabilized
362 by β -lactoglobulin at different ionic strengths (i.e. 10 and 200 mM) were determined. An
363 increase of the ionic strength resulted in an increase of the average droplet size and decay
364 time measured by static light scattering (SLS) and DWS, respectively (figures 5A and B).
365 The increase of the droplet size is also reflected in a shift of the transition between the
366 protein-poor and protein-rich regime from $\sim 2 \text{ g L}^{-1}$ at 10 mM to $\sim 2.5 \text{ g L}^{-1}$ at 200 mM.
367 The effect of ionic strength was expected since the maximum adsorbed amount (Γ_{max})
368 increases with ionic strength as a result of a decrease of the effective radius (R_{eff})
369 (equation 6). This is confirmed by the fact that the curves superimpose when the data is
370 corrected by $\Gamma_{\text{mono, theory}}$ according to equation 4 (figure 5C). As observed for the different
371 proteins, F_{s} equals 2.

372

373

374 3.3. *Application of the surface coverage model*

375 As described above, for different proteins and at different ionic strength, the graph of $d_{3,2}$
376 as a function of $C(1 - \Phi_{oil})Q_H/6\Phi_{oil}\Gamma_{mono, theory}$ shows a point where the emulsions reach the
377 stable regime ($d_{3,2} = d_{3,2, min}$) (i.e. $C_{cr} = 2$). This point is named the stability factor (F_s) and
378 has a value of 2 for all experiments. This shows that equation 3 can be applied to predict
379 the droplet size for the obtained experimental data, when the stability factor of 2 is
380 included (equation 12).

$$d_{3,2} = \frac{F_s 6\Phi_{oil}\Gamma_{mono, theory}}{(1 - \Phi_{oil})Q_H C} \quad (12)$$

381 In the current state, equation 12 is only a first order approximation describing the stability
382 of emulsions as affected by ionic strength and concentration. Consequently, it needs
383 further development (e.g. rationalization of the approach and validation for different
384 conditions such as pH and Φ_{oil}). Still, the proposed model can be applied to other
385 proteins, concentrates and isolates at different conditions (e.g. ionic strength, Φ_{oil}).
386 Therefore, experimental data ($d_{3,2}$ as function of concentration) was collected from
387 literature [5, 20, 23, 56]. Subsequently, the curves of the droplet size under these
388 conditions were predicted using equations 2 and 12 assuming that Γ_{max} equals $\Gamma_{mono, theory}$
389 (equation 4) [14]. In addition, a Q_H of 0.73 for patatin [20] and 1.00 for whey protein
390 isolate and concentrate (i.e. equal to β -lactoglobulin) were used (figure 6). The theoretical
391 predictions of $d_{3,2}$ were in good agreement with the experimental results. This shows that
392 even in the current form, the model already shows a quite good quantitative
393 approximation of real, experimental data.

394

395

396 3.4. Predicting emulsion stability

397 Using the current model (i.e. so far approximating k_{adsorb} by Q_H), the critical protein
398 concentration (C_{cr}) that separates the protein-poor from the protein-rich regime can be
399 calculated for any protein under any condition using equation 13.

$$C_{cr} = \frac{F_s 6\Phi_{oil} \Gamma_{mono,theory}}{(1 - \Phi_{oil}) Q_H d_{3,2,min}} \quad (13)$$

400 The current model, as described in equation 13, only considers coalescence and
401 flocculation as possible destabilization mechanism. In practice, creaming also plays an
402 important role. The creaming rate of emulsion droplets (v [$m\ s^{-2}$]) can be approximated by
403 Stokes' law (equation 14).

$$v = \frac{2(\rho_d - \rho_c)gR^2}{9\eta_c} \quad (14)$$

404 where ρ_d and ρ_c are the mass density of dispersed and continuous phase, respectively [kg
405 m^{-3}], g is gravitational acceleration [$9.80665\ m\ s^{-2}$], R is the radius of the emulsion
406 droplet [m] and η_c is the viscosity of the continuous phase [$kg\ s^{-1}\ m^{-1}$].

407 If the creaming rate is in the order of 1 mm per day, creaming is considered negligible
408 [57]. Therefore, the stability of an emulsion against destabilization can be predicted by
409 combing equations 13 and 14 with a creaming rate of 1 mm/day (equation 15).

$$C_{cr} = \frac{F_s 6\Phi_{oil} \Gamma_{mono,theory}}{(1 - \Phi_{oil}) Q_H 2\sqrt{\frac{1.16 \cdot 10^{-8} \cdot 9\eta_c}{2(\rho_d - \rho_c)g}}} \quad (15)$$

410

411 **4. CONCLUSIONS**

412 The stability of emulsions during formation is found to be affected by the same factors as the
413 stability against flocculation after changes in conditions. In both cases, the stability is determined

414 by the coverage of the interface. A completely covered interface increases the stability against
415 coalescence and flocculation. In addition to parameters related to the adsorbed layer (i.e.
416 maximum adsorbed amount and interfacial area), the adsorption kinetics also affected the
417 stability of the emulsion. Based on this information, the surface coverage model is proposed. The
418 proposed model describes experimental data (i.e. droplet size) quantitatively and can therefore be
419 used as a guideline to develop a more extended model for predicting the behaviour of protein-
420 stabilized emulsions under different system conditions (i.e. pH and Φ_{oil}).

421

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426 **Notes**

427 The authors declare no competing financial interest.

428

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539

540 **TABLES**541 **Table 1.** Protein properties obtained from literature.542

Protein	M_w^a [kDa]	Q_H^b [-]	$\Gamma_{\text{mono,theory}}^b$ [mg m ⁻²]	ζ Potential ^b [mV]
β -Lactoglobulin	18.3	0.52	1.62 ^c	-21.2
Ovalbumin	42.8	0.10	1.73	-16.5
Lysozyme	14.3	0.03	1.58	2.0

543 ^avalues obtained from the Swiss-Prot database (<http://www.expasy.org>). ^bliterature values[14]. ^c $\Gamma_{\text{mono,theory}}$ 544 for a β -lactoglobulin dimer.

545

546 **FIGURE CAPTIONS**

547 **Figure 1.** Effect of low and high protein concentration on the emulsion stability against
548 coalescence during formation (A) and against flocculation after formation (B). The dark and light
549 grey circles represent the protein and the Debye screening length, respectively. The effective
550 radius of an adsorbed protein is a combination of protein and the Debye screening length.

551
552 **Figure 2.** Average droplet size ($d_{3,2}$) as function of protein concentration (A) and as function of
553 $C(1-\Phi_{oil})/6\Phi_{oil}\Gamma_{max}$ (B) calculated from equation 1 with a $d_{3,2, min}$ of 1 μm (equation 2) for
554 emulsions with $\Phi_{oil} = 0.2$ and $\Gamma_{max} = 3 \text{ mg m}^{-2}$ (1), $\Phi_{oil} = 0.2$ and $\Gamma_{max} = 5 \text{ mg m}^{-2}$ (2) and $\Phi_{oil} =$
555 0.4 and $\Gamma_{max} = 3 \text{ mg m}^{-2}$ (3). The grey area in figure B represents the protein-poor regime.

556
557 **Figure 3.** Decay time ($\tau_{1/2}$) as a function of the absolute zeta potential for emulsion droplets
558 stabilized by β -lactoglobulin at 2 g L^{-1} (\diamond), 5 g L^{-1} (\square), and 2 g L^{-1} supplemented to a
559 concentration of 5 g L^{-1} (\circ) ($\text{pH} = 7.0$ and $\Phi_{oil} = 0.1$). The solid lines are guides to the eye.

560
561 **Figure 4.** Decay time ($\tau_{1/2}$) (A) and average droplet size ($d_{3,2}$) (B) as function of protein
562 concentration and average droplet size as function of $C(1-\Phi_{oil})/6\Phi_{oil}\Gamma_{max}$ (C) and as function of
563 $C(1-\Phi_{oil})Q_H/6\Phi_{oil}\Gamma_{max}$ (D) for emulsions stabilized by β -lactoglobulin (\diamond), ovalbumin (\triangle) and
564 lysozyme (\square) ($\text{pH} = 7.0$, $I = 10 \text{ mM}$ and $\Phi_{oil} = 0.1$). The grey area in figure D represents the
565 protein-poor regime. The inserts show the small droplet size regime. Lines are guides to the eye.

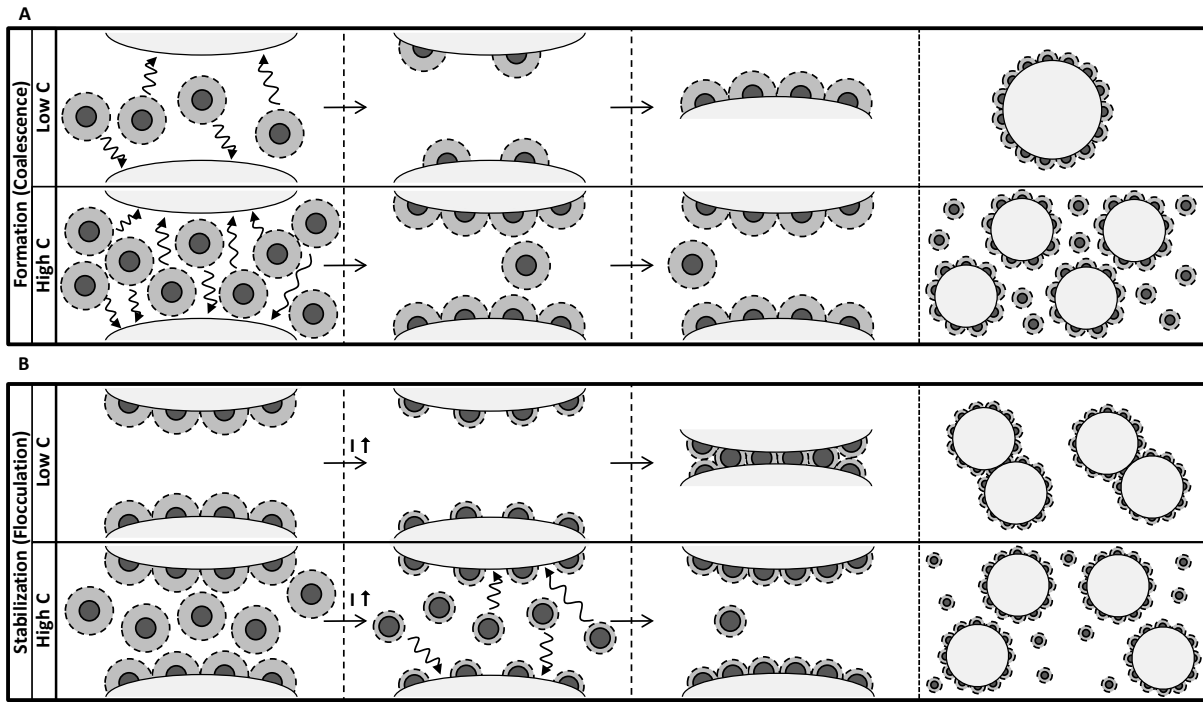
566
567 **Figure 5.** Concentration dependence of the decay time ($\tau_{1/2}$) (A), average droplet size ($d_{3,2}$) (B)
568 and average droplet size as function of $C(1-\Phi_{oil})Q_H/6\Phi_{oil}\Gamma_{mono,theory}$ (C) for

569 β -lactoglobulin-stabilized emulsions at an ionic strength of 10 mM (\diamond) and 200 mM (\triangle) (pH =
570 7.0 and $\Phi_{oil} = 0.1$). The grey areas in A and B represent the protein-poor regime at ionic strength
571 of 10 (light grey) and 200 mM (dark grey). The grey area in C represents the protein-poor
572 regime. The inserts show the small droplet size regime.

573

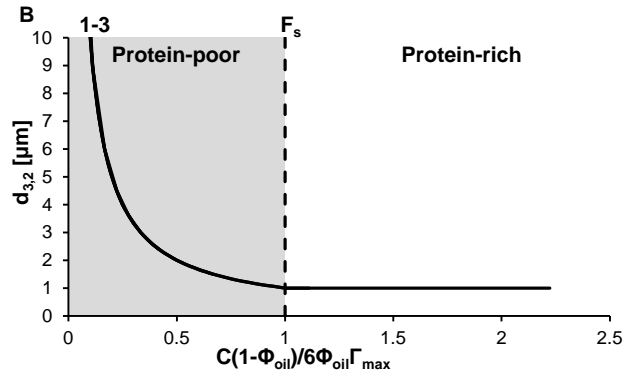
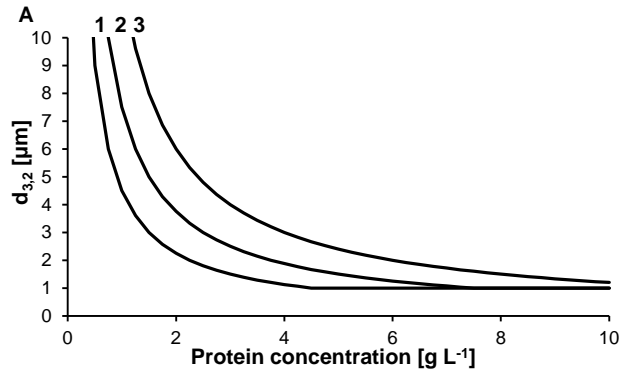
574 **Figure 6.** Average droplet size ($d_{3,2}$) for emulsions stabilized by β -lactoglobulin (pH = 7.0, I =
575 10 mM and $\Phi_{oil} = 0.1$)[20] (A), patatin (pH = 7.0, I = 50 mM and $\Phi_{oil} = 0.1$)[56] (B), whey
576 protein isolate (pH = 7.0, I = 10 mM and $\Phi_{oil} = 0.3$)[23] (C) and whey protein concentrate (pH =
577 7.0, I = 150 mM and $\Phi_{oil} = 0.28$)²¹ (D). The dashed lines represent the fit of the data using
578 equations 2 and 3, with $k_{adsorb} = Q_H$.

579



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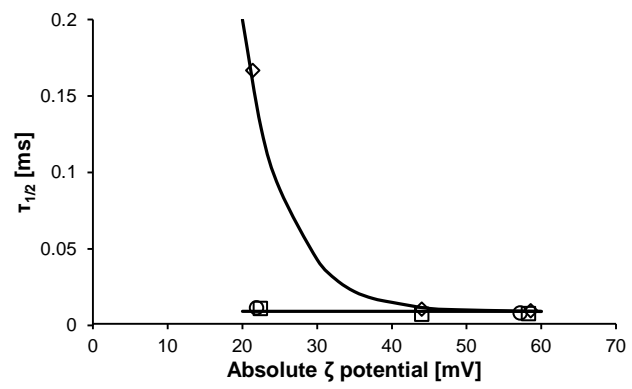
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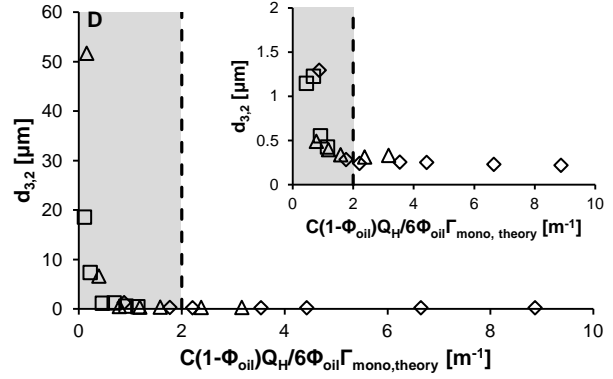
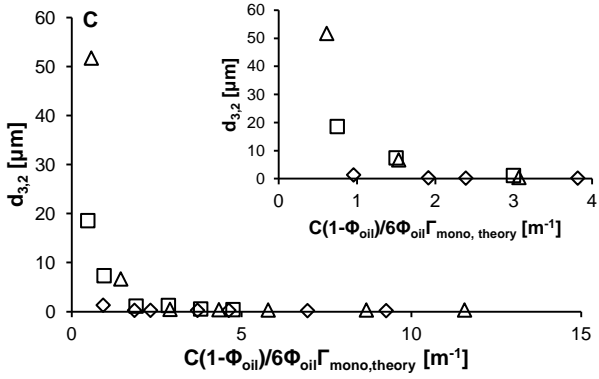
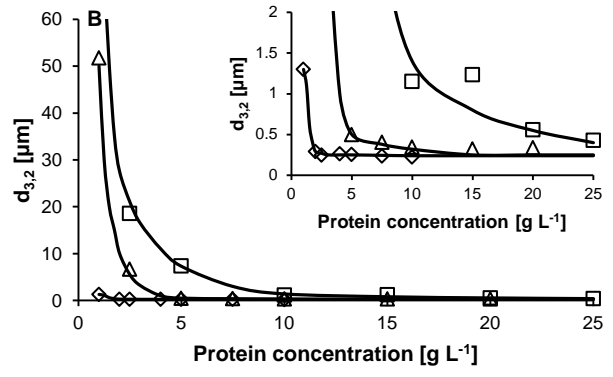
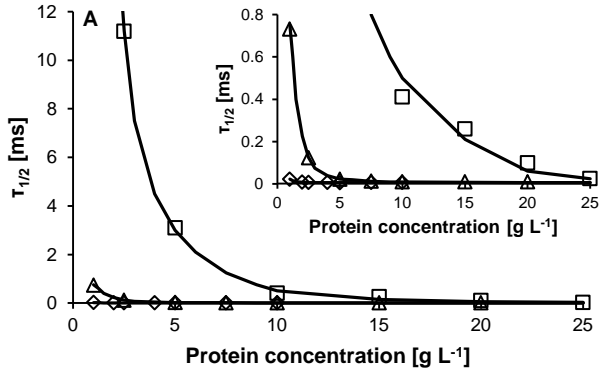


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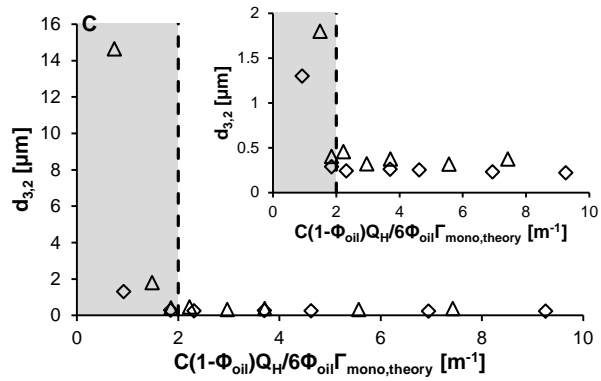
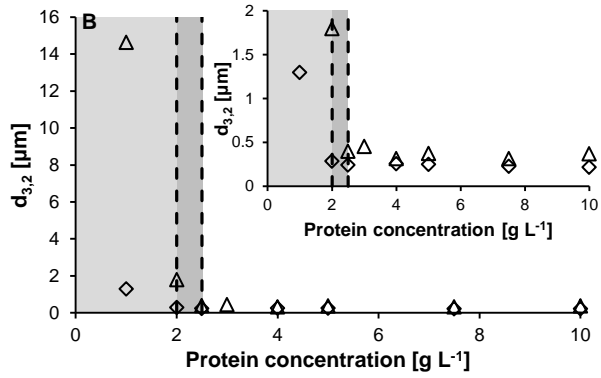
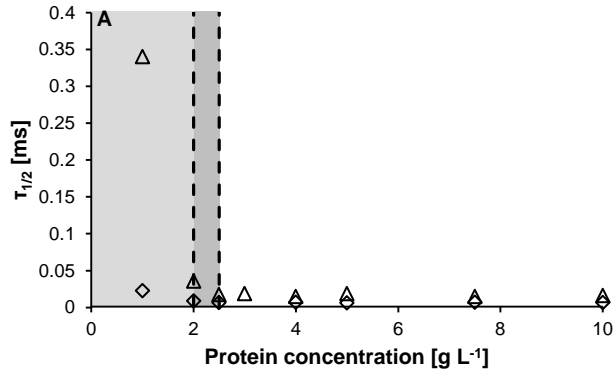
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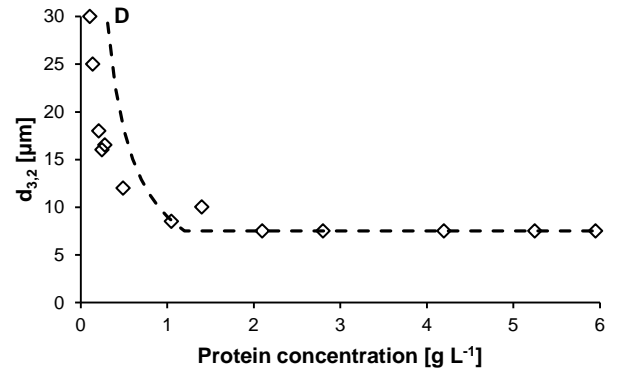
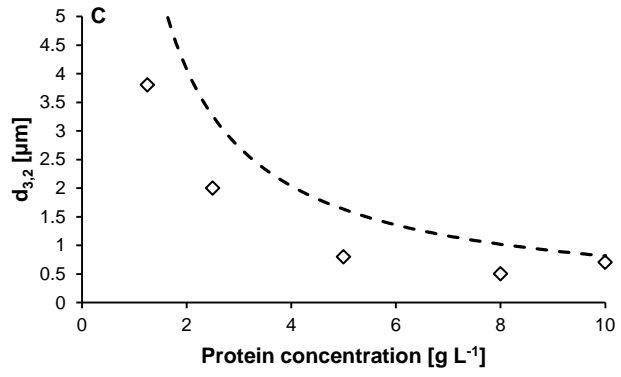
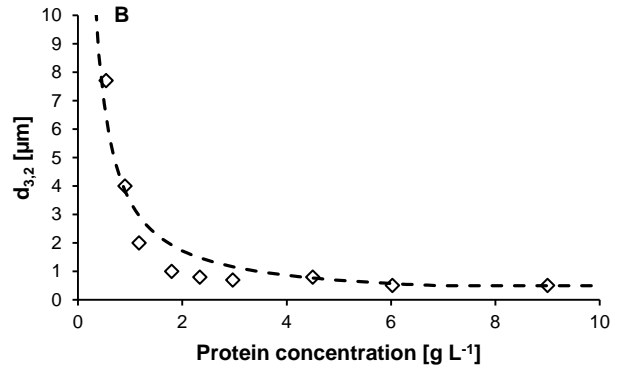
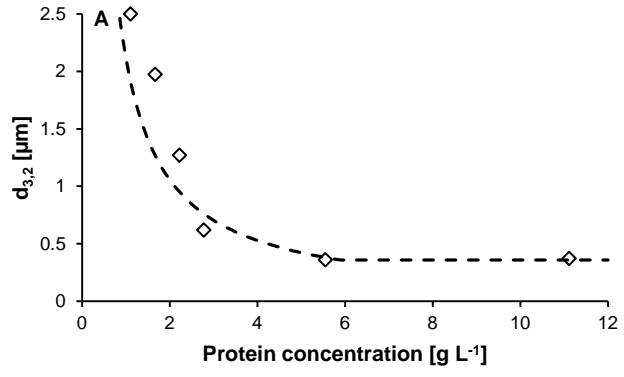
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